# Comsol Conference 2008 Nonlinear Ferrohydrodynamics of Magnetic Fluids

Markus Zahn Massachusetts Institute of Technology Department of Electrical Engineering and Computer Science Laboratory for Electromagnetic and Electronic Systems

# OUTLINE

- 1. Introduction to Ferrohydrodynamics
- 2. Applications to Magnetic Resonance Imaging (MRI)
- 3. Applications to Increasing Power Transformer Electric Breakdown Strength
- 4. Ferrohydrodynamic Instabilities
- 5. Dielectric Analog: Von Quincke Electrorotation

## 1. INTRODUCTION TO FERRODYNAMICS

#### FERROHYDRODYNAMICS

$$\overline{F} = \begin{cases} \overline{J} \times \overline{B} - \frac{1}{2} H^2 \nabla \mu & (\mathbf{I} \\ \overline{J} \times \mu_0 \overline{H} + \mu_0 (\overline{M} \bullet \nabla) \overline{H} & (\mathbf{I} \\ \tau = \sigma \mu \ell^2 & (\mathbf{I} \\ \mathbf{I} \end{pmatrix}$$

(Linear Magnetization)

(Force Density)

H (Magnetizable Medium)

(Magnetic Diffusion Time)

$$\delta = \sqrt{\frac{2}{\omega\mu\sigma}}$$

(Skin Depth)

$$R_m = \frac{\sigma \mu \ell^2}{\ell / \nu} = \sigma \mu \nu \ell$$

(Magnetic Reynolds Number)

#### ELECTROHYDRODYNAMICS

$$\overline{F} = \begin{cases} \rho_f \overline{E} - \frac{1}{2} E^2 \nabla \varepsilon & \text{(Linear Dielectric)} \\ \rho_f \overline{E} + (\overline{P} \bullet \nabla) \overline{E} & \text{(Polarizable Dielectric)} \\ \tau = \varepsilon / \sigma & \text{(Dielectric Relaxation Time)} \\ R_e = \frac{\varepsilon / \sigma}{\ell / \nu} = \frac{\varepsilon \nu}{\sigma \ell} & \text{(Electric Reynolds Number)} \end{cases}$$

# Ferrofluids

Colloidal dispersion of permanently magnetized particles undergoing rotational and translational Brownian motion.

Established applications

rotary and exclusion seals, stepper motor dampers, heat transfer fluids

Emerging applications MEMS/NEMS – motors, generators, actuators, pumps Bio/Medical – cell sorters, biosensors, magnetocytolysis, targeted drug delivery vectors, *in vivo* imaging, hyperthermia, immunoassays Separations – magneto-responsive colloidal extractants



## **Ferrofluid Magnetic Properties**



Water-based Ferrofluid  $\mu_0 M_s = 203 \text{ Gauss}$   $\phi = 0.036$ ;  $\chi_0 = 0.65$ ,  $\rho = 1.22 \text{ g/cc}$ ,  $\eta \approx 7 \text{ cp}$   $d_{\min} \approx 5.5 \text{ nm}$ ,  $d_{\max} \approx 11.9 \text{ nm}$  $\tau_B = 2-10 \text{ }\mu\text{s}$ ,  $\tau_N = 5 \text{ ns-}20 \text{ ms}$  lsopar-M Ferrofluid μ<sub>0</sub>M<sub>s</sub> = 444 Gauss φ = 0.079 ; χ<sub>0</sub> = 2.18, ρ=1.18 g/cc, η≈11 cp d<sub>min</sub>≈7.7 nm, d<sub>max</sub>≈13.8 nm τ<sub>B</sub>=7-20 μs, τ<sub>N</sub>=100 ns-200 s

Langevin Equation 
$$\left[\frac{M}{M_s} = \coth \alpha - \frac{1}{\alpha}\right]$$



Measured magnetization (dots) for four ferrofluids containing magnetite particles ( $M_d = 4.46 \times 10^5$  Ampere/meter or equivalently  $\mu_o M_d = 0.56$  Tesla) plotted with the theoretical Langevin curve (solid line). The data consist of Ferrotec Corporation ferrofluids: NF 1634 Isopar M at 25.4° C, 50.2° C, and 100.4° C all with fitted particle size of 11 nm; MSG W11 water-based at 26.3° C and 50.2° C with fitted particle size of 8 nm; NBF 1677 fluorocarbon-based at 50.2° C with fitted particle size of 13 nm; and EFH1 (positive  $\alpha$  only) at 27° C with fitted particle size of 11 nm. All data falls on or near the universal Langevin curve indicating superparamagnetic behavior.

## **Characteristic Brownian and Néel Relaxation Times**





The ferrofluid time constant,  $\tau$ , is due to either the Néel  $(\tau_N)$  or Brownian  $(\tau_B)$  relaxation times, depending on the particle's radius.

 $\tau \Box 10^{-6} \,\mathrm{s}$  (7-8 nm water-based magnetite)

## **Ferrofluid Magnetization Force**



A magnetizable liquid is drawn upward around a current-carrying wire.

# 2. Application of Magnetic Media to Magnetic Resonance Imaging (MRI)



The fundamental elements of MRI are (a) dipole alignment, (b) RF excitation at Larmor frequency  $f = \gamma B_0 / 2\pi$ , (c) slice selection and (d) image reconstruction.

maginal signal signal signal time time

T2 decay is characterized by the exponential decay envelope of the magnetization signal in the  $\{xy\}$  plane after excitation. T1 recovery is characterized by the exponential growth of the magnetization along the z axis as the vector returns to the equilibrium magnetization.

Larmor Frequency  $f = \gamma B_0 / 2\pi = 42.576 \text{ MHz/Tesla for Protons}$ ( $\gamma = \text{gyromagnetic ratio}, \frac{\gamma}{2\pi} = 42.576 \text{ MHz/Tesla for }^{1}H \text{ nucleus.}$ )

# Ferrofluids as Contrast Agents in MRI

MRI Image of the Brain (A) Before and (B) After Gadalinium contrast enhancement



Two categories of contrast agents in MRI:

- Ferrofluids called superparamagnetic iron oxide (SPIO) contrast agents (currently smaller market share)
- Gadolinium-based contrast agents

T1 weighted MRI of the brain (a) before and (b) after Gadolinium contrast enhancement, showing a metastatic deposit involving the right frontal bone with a large extracranial soft tissue component and meningeal invasion. This figure comes from a case report of suspected dormant micrometatasis in a cancer patient.

## Effect of Ferrofluid on Image Contrast



 $A: \phi = 4.7 \times 10^{-7}$  $\phi$  =Percentage $F: \phi = 1.4 \times 10^{-5}$ solid volumeExperiments at the Martinos Center forBiomedical Imaging (MGH)

Vial	Solid Volume Fraction, $\phi$	T1 in ms	T2 in ms
Α	$4.7 \times 10^{-7}$	1706	265
В	$1.15 imes10^{-6}$	1345	108
С	$2.2 \times 10^{-6}$	1009	74
D	$2.75 imes10^{-6}$	887	57
E	$5.5  imes 10^{-6}$	-	27
F	$1.4 \times 10^{-5}$	-	20

T1 and T2 results for various water based ferrofluid solid volume fractions,  $\phi$ . At very high concentrations ( $\phi$ >5 x 10<sup>-6</sup>), the SNR was not sufficient to allow for the accurate determination of T1 relaxation times.

Pádraig Cantillon-Murphy, "On the Dynamics of Magnetic Fluids in Magnetic Resonance Imaging", Massachusetts Institute of Technology PhD thesis, May 2008.

# T2 Time Constant as Function of Ferrofluid Solid Volume Fraction $\phi$



Comparison of the theoretical prediction for T2 at various superparamagnetic particle radii with the experimental results over a range of MSG W11 water-based ferrofluid concentrations of the original 2.75% solution by volume.

#### Ferrofluid Contribution to MRI Relaxation Time, T2

T2 Dependence on Ferrofluid Concentration



Pádraig Cantillon-Murphy, "On the Dynamics of Magnetic Fluids in Magnetic Resonance Imaging", Massachusetts Institute of Technology PhD thesis, May 2008.

# **Conservation of Linear and Angular Momentum**

$$0 = \rho \mathbf{g} + \mu_0 \mathbf{M} \cdot \nabla \mathbf{H} - \nabla p + (\eta + \zeta) \nabla^2 \mathbf{v} + 2\zeta \left( \nabla \times \boldsymbol{\omega} \right)$$



- Viscous dominated regime
- Particle spin-velocity is no longer given by vorticity
- Magnetic torque density in Con of Ang Mom:

 $0 = \mu_0 \mathbf{M} \times \mathbf{H} + 2\zeta \left( \nabla \times \mathbf{v} - 2\dot{\boldsymbol{\omega}} \right)$ 

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- $N = num. particles per m^3$
- $\zeta$  = vortex viscosity
- n = kinematic viscosity

## Effect of Spin-velocity on Dynamics



- M and H are related by a complex susceptibility
  - $-\Omega$  (electrical frequency)
  - $-\tau$  (ferrofluid time constant)
  - $-\omega$  (spin-velocity)
  - v (flow velocity)

$$\frac{\mathbf{M}}{\partial t} + (\mathbf{v} \bullet \nabla)\mathbf{M} - \boldsymbol{\omega} \times \mathbf{M} = -\frac{1}{\tau} (\mathbf{M} - \mathbf{M}_{eq})$$

Comsol Problem Definition

## **Concentric Cylinders of Water and Ferrofluid**



# Complex Susceptibility

• Relating small-signal magnetic field to small-signal ferrofluid magnetization

$$\frac{\partial \mathbf{M}}{\partial t} + (\mathbf{v} \cdot \nabla) \mathbf{M} - \mathbf{\omega} \times \mathbf{M} = -\frac{1}{\tau} (\mathbf{M} - \mathbf{M}_{eq}) \xrightarrow{Xy} \mathbf{m} = \mathbf{\chi} \mathbf{h}$$

$$\begin{pmatrix} \mathbf{m}_{x} \\ \mathbf{m}_{y} \end{pmatrix} = \frac{M_{0}}{H_{0}} \begin{pmatrix} (1 + q\mathbf{i}\Omega \mathbf{j}) & (z\tau) \\ -(\omega_{z}\tau) & (1 + j\Omega\tau) \end{pmatrix} \begin{pmatrix} \mathbf{h}_{x} \\ \mathbf{h}_{y} \end{pmatrix}$$

#### Exporting Comsol Results to Matlab Instantaneous transverse B field



### 3. Applications to Increasing Power Transformer Electric Breakdown Strength

#### **Electrical Streamer**

- Streamers are low-density conductive structures that form when dielectric liquids are electrically over-stressed [2].
- Streamer characteristics are polarity dependent.
  - Positive Excitation: Filamentary structure, Breakdown velocities greater than 1 km/s, 4 propagation modes.
  - Negative Excitation: Bushy structure, Breakdown velocities greater than 100 m/s, 3 propagation modes.



Positive streamer growth in transformer oil.  $V_{appl}$ = 82 kV, Gap d= 1.27 cm. [3]



Negative streamer growth in transformer oil.  $V_{appl}$  = 82 kV, Gap d= 1.27 cm. [3]

Photos taken from:

J. C. Devins, et al, "Breakdown and Pre-breakdown Phenomena in Liquids," J. Appl. Phys., 52 (7), July 1981.

# **Charge Generation Mechanisms**

- Observable streamer structures are the result of electrically driven thermal dissipation.
- □ The role of four charge generation mechanisms have been explored.
  - Fowler-Nordheim electron injection (Unimportant)
    - Injection of electrons from a highly stressed negative electrode.
  - Electric field assisted ionic dissociation (Unimportant)
    - Generation of positive and negative ions due to dissociation of weakly bonded neutral ion-pairs at high electric fields.
  - Impact ionization (Unimportant)
    - Generation of positive ions and electrons due to inelastic collisions of free electrons that are accelerated in the high electric field levels.
  - Electric field dependent molecular ionization, Field ionization (Most Important)
    - Generation of positive ions and electrons due to the direct ionization of neutral molecules at high electric field levels.

#### Nanoparticle Charging Dynamics

 As a nanoparticle captures charge the electric field distribution in the vicinity of the particle changes with a decreasing charge capture window

$$Q(t) = \frac{Q_s}{1 + \frac{4t}{\tau}}, \quad Q_s = 12\pi\varepsilon E_0 R^2, \quad \tau = \frac{\varepsilon}{\rho_0 \mu}$$



## **Electrodynamic Model for Nanofluid**

- The trapping of electrons by nanoparticles in a nanofluid can be modeled by adding an attachment term to both the electron and negative ion continuity equations
- Heaviside function  $H(\rho_{NPsat} \rho_{-})$  is used to account for the charge saturation of the nanoparticles
- Consider a 1 Gauss ferrofluid manufactured using 10 (nm) diameter particles:  $n_0 = 3.4 \times 10^{20} (1/\text{m}^3)$

$$\begin{aligned} -\nabla \cdot (\varepsilon \nabla V) &= \rho_{+} + \rho_{-} + \rho_{e} \quad \text{where} \quad \vec{E} = -\nabla V \\ \frac{\partial \rho_{+}}{\partial t} + \nabla \cdot \vec{J}_{+} &= G_{I}(|\vec{E}|) + \frac{\rho_{+}\rho_{e}R_{+/e}}{e} + \frac{\rho_{+}\rho_{-}R_{\pm}}{e} \\ \frac{\partial \rho_{e}}{\partial t} + \nabla \cdot \vec{J}_{e} &= -G_{I}(|\vec{E}|) - \frac{\rho_{+}\rho_{e}R_{+/e}}{e} - \frac{\rho_{e}}{\tau_{a}} - \frac{\rho_{e}}{\tau_{NP}} (1 - H(\rho_{NPsat} - \rho_{-})) \\ \frac{\partial \rho_{-}}{\partial t} + \nabla \cdot \vec{J}_{-} &= \frac{\rho_{e}}{\tau_{a}} - \frac{\rho_{+}\rho_{-}R_{\pm}}{e} + \frac{\rho_{e}}{\tau_{NP}} (1 - H(\rho_{NPsat} - \rho_{-})) \\ G_{I}(|\vec{E}|) &= A_{f} |\vec{E}| \exp\left(-\frac{B_{f}}{|\vec{E}|}\right) \quad \Rightarrow \quad A_{f} = \frac{e^{2}n_{0}a}{h} \quad B_{f} = \frac{\pi^{2}m^{*}a\Delta^{2}}{eh^{2}} \end{aligned}$$

## **Electric Field Dynamics in Nanofluids**

Simulations using nanoparticle attachment time constant values ( $\tau_{NP}$ ) of 2, 5 and 50 (ns)



# **Results: Surface Electric Field**



• Field ionization results in the development of a moving dissipative source that "sweeps" through the oil.





# 4. Ferrohydrodynamic Instabilities In DC Magnetic Fields

# Labyrinthine Instability in Magnetic Fluids





Magnetic fluid in a thin layer with uniform magnetic field applied tangential to thin dimension. Stages in magnetic fluid labyrinthine patterns in a vertical cell, 75 mm on a side with 1 mm gap, with magnetic field ramped from zero to 535 Gauss.

## **Rotating Magnetic Fields**



Observed magnetic field distribution in the 3 phase AC stator



Ferrofluid Drops in Rotating Magnetic Fields



## Ferrofluid Spiral / Phase Transformations



## 5. Dielectric Analog: Von Quincke's Rotor (Electrorotation)



(a) Von Quincke's rotor consists of a highly insulating cylinder that is free to rotate and that is placed in slightly conducting oil between parallel plate electrodes. As DC high voltage is raised, at a critical voltage the cylinder spontaneously rotates in either direction; (b) The motion occurs because the insulating rotor charges like a capacitor with positive surface charge near the positive electrode and negative surface charge near the negative electrode. Any slight rotation of the cylinder in either direction results in an electrical torque in the same direction as the initial displacement.

## **Electrorotation**—Introduction

Experiments have shown that for a given pressure gradient, the Poiseuille flow rate can be increased (Lemaire et al., 2006) by introducing micro-particle electrorotation into the fluid flow via the application of an external direct current (DC) electric field.



### **Electrorotation**—Quincke rotation

The electric torque 
$$\overline{T_e} = \overline{p} \times \overline{E} = \frac{6\pi\varepsilon_1 R^3 E_0^2 (1 - \tau_1/\tau_2) \Omega \tau_{MW}}{(1 + 2\varepsilon_1/\varepsilon_2) (1 + \sigma_2/2\sigma_1) (1 + \Omega^2 \tau_{MW}^2)}$$

For a small perturbation of rotation to grow, the torque balance on the particle is rewritten as (Jones, 1995):

$$I\frac{d\Omega}{dt} = \left[\frac{6\pi\varepsilon_1 R^3 E_0^2 \left(1 - \tau_1/\tau_2\right)\Omega \tau_{MW}}{\left(1 + 2\varepsilon_1/\varepsilon_2\right)\left(1 + \sigma_2/2\sigma_1\right)\left(1 + \Omega^2 \tau_{MW}^2\right)} - 8\pi\eta_1 R^3\Omega\right]$$

The bracket term should have a value larger than zero for the small perturbation to grow (Jones, 1995), thus

$$\tau_2 > \tau_1$$

## **Electrorotation**—Quincke rotation

