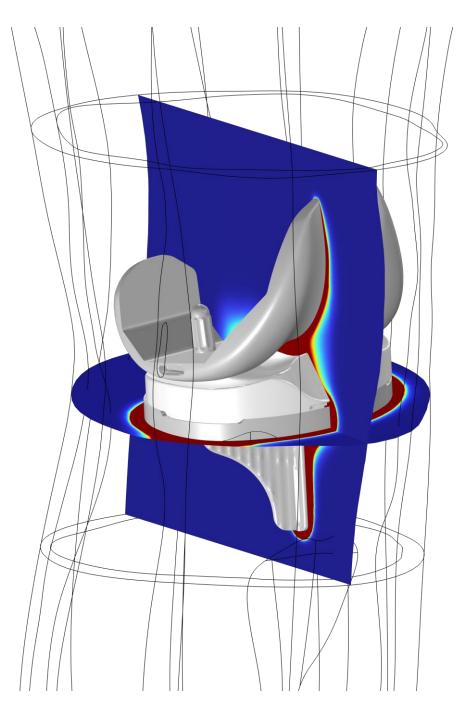
# **Electromagnetic Heating Simulation of Medical Treatment for Infections After Knee Replacement** Surgery

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Bibin Prasad, John Tepper, and Rajiv Chopra from Solenic Medical





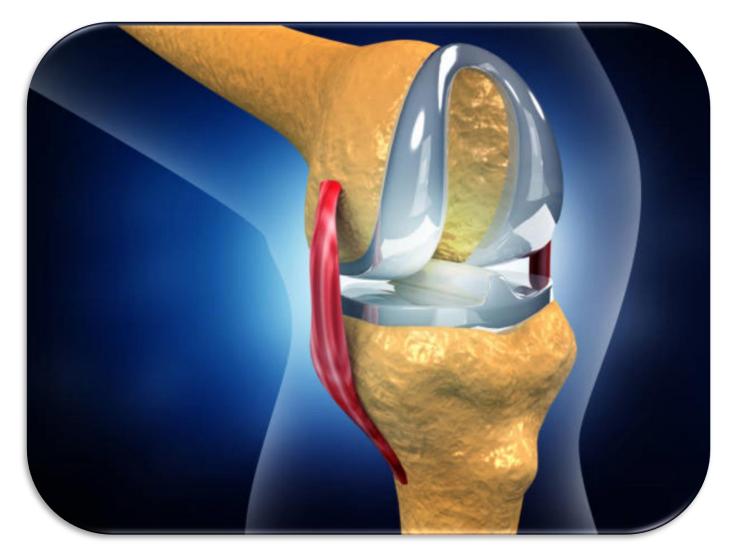
Introduction

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#### **Project Challenge**



Develop a device to therapeutically treat knee replacements



### **Project Situation**





- Start-up medical device company
- Identified significant medical issue
- Needed
  - Successful first physical prototyping
  - FDA approval of design
- Customer lacked internal simulation capabilities

#### **PROJECT GOALS:**

- 1. Rapidly show proof of concept
- 2. Model to support FDA approval of the device



#### Methods and use of COMSOL Multiphysics<sup>®</sup>

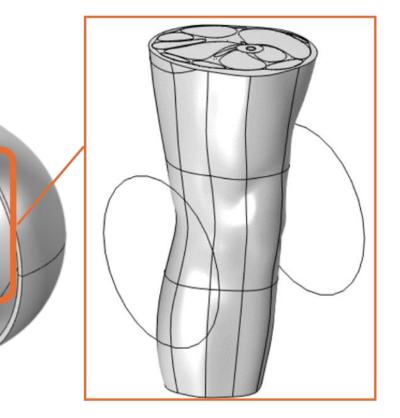




- Current in a Helmholtz coil excites heating of implant metal
- Temperatures near metal implants provide therapeutic benefit
- Quantification of damage in tissue is critical for FDA

#### Geometry

- Magnetic fields physics included in all regions including spherical air space around knee
- Helmholtz coils on either side of knee
- Surgically replaced knee joint and surrounding tissue from mid-calf to mid-thigh



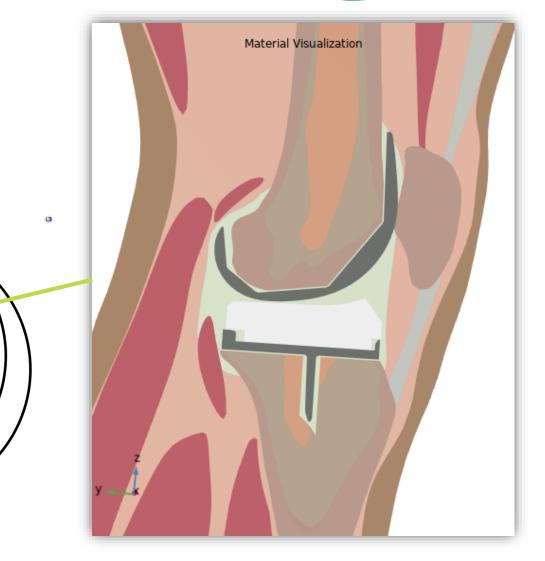


### **Detailed Anatomical Model**

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- Individual tissues included
- Femoral, tibial metal implant
- Plastic insert





### **Bioheat Physics Included**

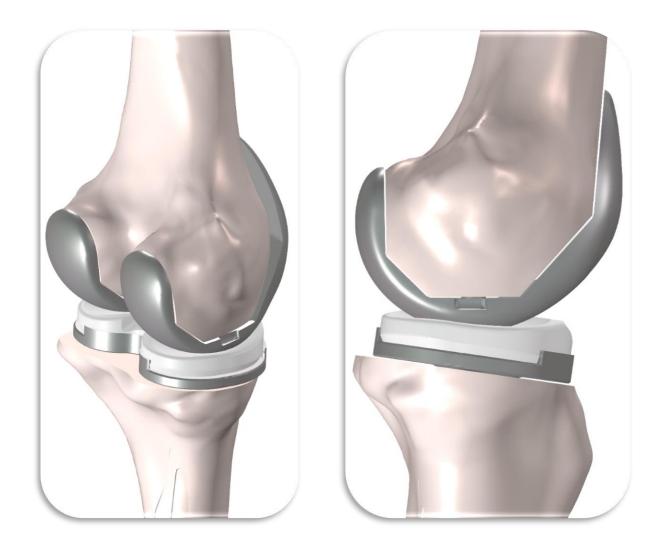


 Blood perfusion rate and Metabolic heat source specific to tissue type

Image: BioheatArterial blood temperature: $T_b$ $T_blood$ $K_b$ Specific heat, blood: $C_{p,b}$ $Cp_blood$ $J/(kg·K)$ Blood perfusion rate: $\omega_b$ perfusion $1/s$ Density, blood:
$T_b$ T_bloodKSpecific heat, blood: $C_{p,b}$ $C_{p,b}$ Cp_bloodBlood perfusion rate: $J/(kg\cdot K)$ $\omega_b$ perfusion1/s
Specific heat, blood:       C <sub>p,b</sub> Cp_blood       J/(kg·K)       Blood perfusion rate:       ω <sub>b</sub> perfusion       1/s
C <sub>p,b</sub> Cp_blood     J/(kg·K)       Blood perfusion rate:     ω       ω <sub>b</sub> perfusion     1/s
Blood perfusion rate: $\omega_{\rm b}$ perfusion 1/s
ω <sub>b</sub> perfusion 1/s
Density blood:
Density, Diodal
$\rho_{\rm b}$ rho_blood kg/m <sup>3</sup> Spacific to tissue type
Metabolic heat source: O O metabolic heat source: Specific to tissue type from the literature
Q <sub>met</sub> Q_m W/m <sup>3</sup> from the literature

#### **Cement Geometry**





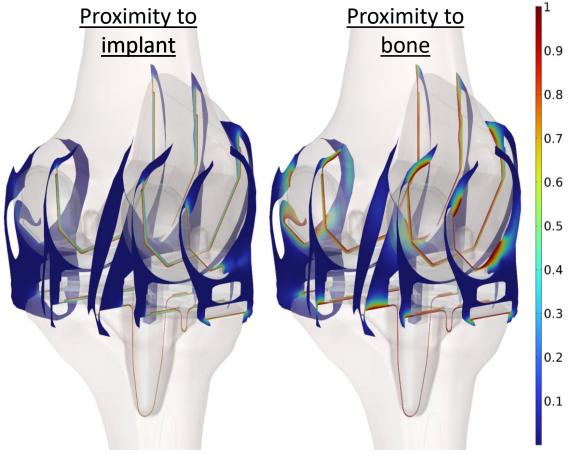
- No CAD for cement regions that provide a permanent surgical connection between metal and bone
- Custom PDE implementation to calculate the extent of cement gap fill between metal and bone

# Used two reaction-diffusion equations to calculate proximity

• PDEs for proximity variables p1 and p2:

 $\nabla \cdot \left[ -(C_1 \cdot h)^2 p_1 \right] = -p_1$  $\nabla \cdot \left[ -(C_2 \cdot h)^2 p_2 \right] = -p_2$ 

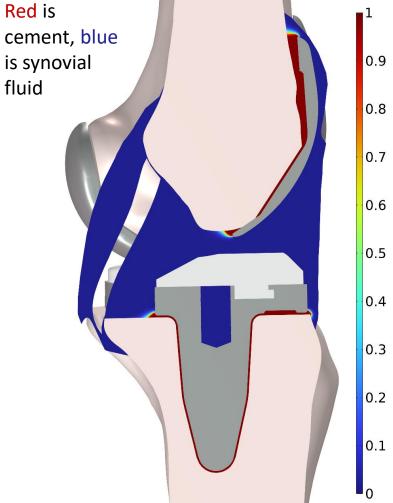
- C<sub>1</sub> and C<sub>2</sub> are smoothing factors on order of 1; h is local element size
- Proximity variables are set to 1 on boundaries that contact cement



# Calculated material properties from proximity variables

- Boolean variable is function of product of proximity variables:
  - Variable definition:  $\varphi = flc1hs(10^{p_1p_2} 1.16, 0.15)$
  - Smooth transition from cement ( $\varphi = 1$ ) to synovial fluid ( $\varphi = 0$ )
  - Expression is arbitrary and visually tuned
- Material properties smoothly transition between cement and synovial fluid: k = k<sub>fluid</sub> + (k<sub>cement</sub> - k<sub>fluid</sub>)φ

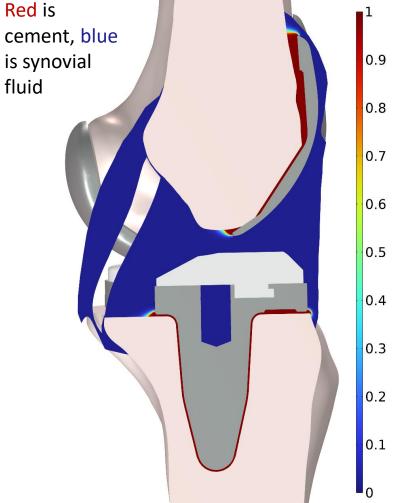




# Calculated material properties from proximity variables

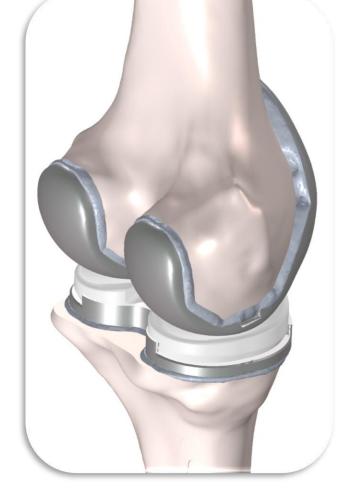
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#### **Approach Produces Cement Distribution**

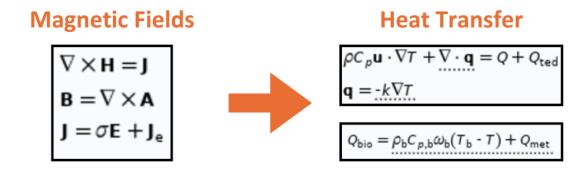
- Cement fills all gaps between bone and implant
- Overfill at edges is relatively small
- Gives good approximation to expected cement distribution from "spread, press, wipe" process used by surgeons





### **Multiphysics Analysis**





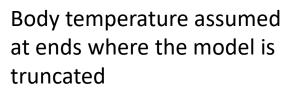
- Magnetic fields interact with metal implants causing heating
- Frequency domain solution simulates heat source
- Transient temperature rise simulated via energy equation with metabolic heating and perfusion cooling effect

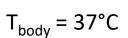
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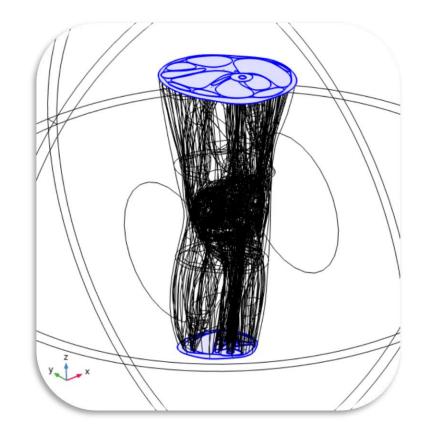
#### **Thermal Boundary Conditions**

Convective heat flux on outside of skin

 $\begin{array}{ll} -\mathbf{n} \cdot \mathbf{q} = \underline{q}_0 & \text{h} = 5 \text{ W/m}^2/\text{K} \\ q_0 = h(\tau_{\text{ext}} - \tau) & T_{\text{ext}} = 30^{\circ}\text{C} \end{array}$ 



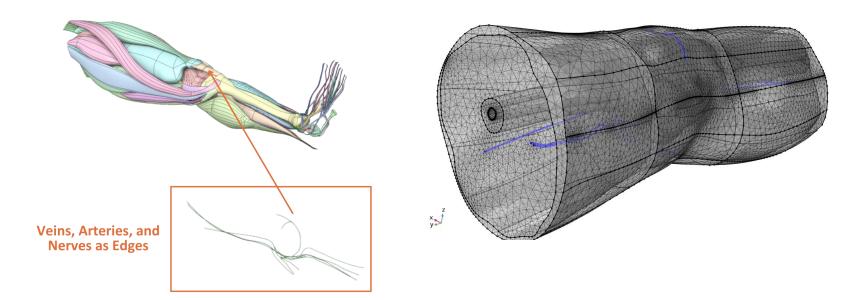






### Arteries, Nerves, and Veins Added as 1D Edges





$$\int_{S(R)}^{Qds} Qds = A_{|}Q_{|} - \nabla_{\mathbf{t}} \cdot A_{|}\mathbf{q}_{|}$$
$$\mathbf{q}_{|} = \frac{-k_{|}\nabla_{\mathbf{t}}T}{\dots}$$
$$A_{|} = \pi r_{|}^{2}$$

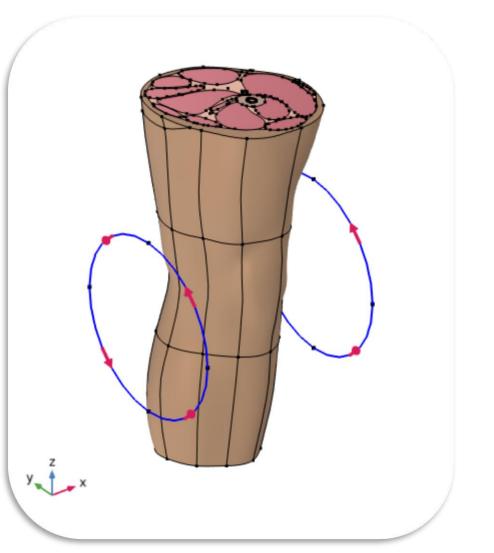
$$\lim_{\partial S \to 0} \int_{\partial S} Q ds = \underline{A_l Q_l} - \nabla_{\mathbf{t}} \cdot A_l \mathbf{q}_l$$

<ul> <li>Line Heat Source</li> </ul>	
Heat source:	
General source	•
Q1 rho_blood*Cp_blood*perfusion*(T_blood-T)+Q_m_edge	W/m³

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## **Physical Loading on System**

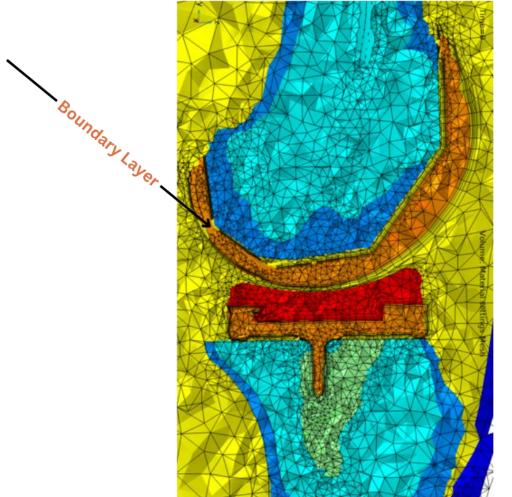
- Helmholtz coil
- Applied current at a specified frequency





#### Meshing





Colors Represent Different Material Regions

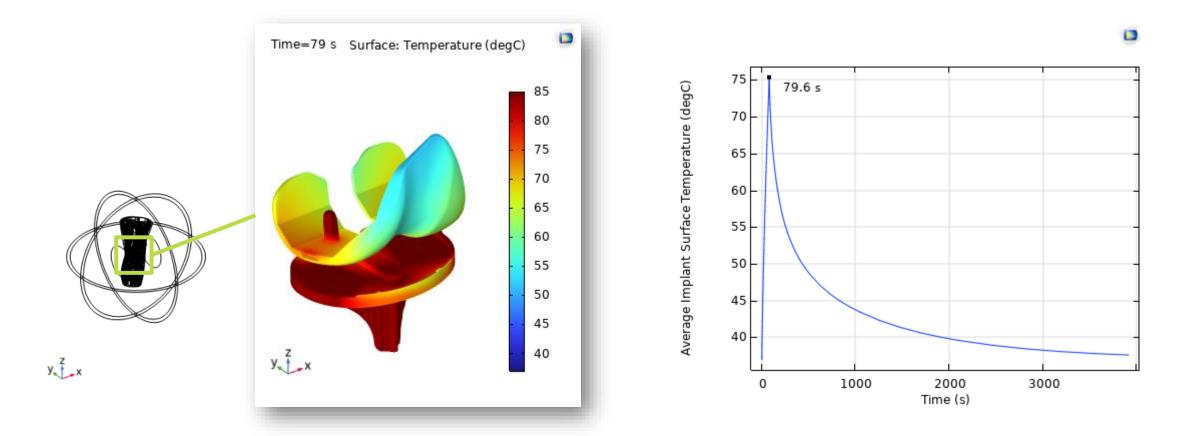
- Free tetrahedral baseline mesh
- Boundary layer mesh added to efficiently discretize field gradients near the implant



Results

#### **Thermal Results**

 Heating occurs for 79.6 seconds then cool down for the remainder of the hour





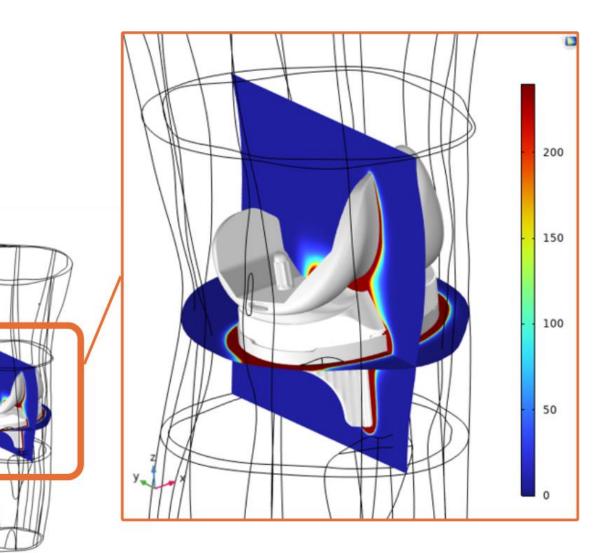
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**Damage Results** 

 Cumulative Equivalent Minutes at 43°C, CEM43

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 Tissue damage after treatment

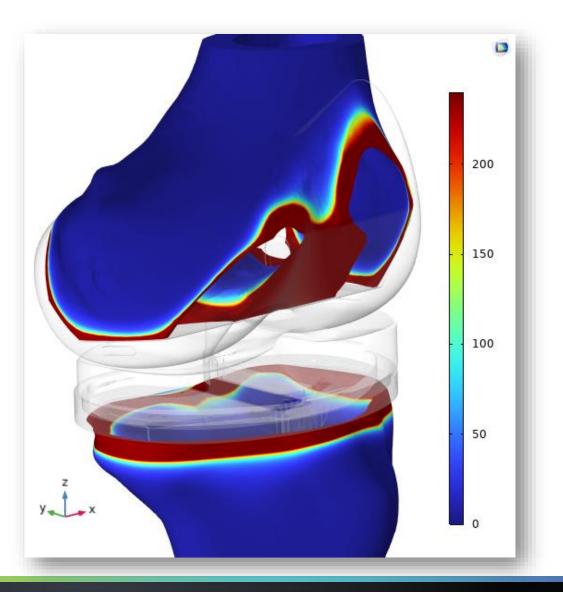




#### **Cortical Bone Damage**



 Damage to the femur and tibia cortical bone





Conclusions

### **AltaSim Technologies' Solution**





- Became simulation team for customer
- Developed simulations that produced workable design
- Provided simulations to customer and trained internal engineers to develop additional simulations

**Customer** – Private equity / device under FDA review





To get in touch call us at (614) 861-7015 or email at info@altasimtechnologies.com or visit https://altasimtechnologies.com/ to learn more.



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